#### WORLD INTELLECTUAL PROPERTY ORGANIZATION International Bureau



#### INTERNATIONAL APPLICATION PUBLISHED UNDER THE PATENT COOPERATION TREATY (PCT)

(51) International Patent Classification 6:		(11) International Publication Number: WO 97/37613
A61F 2/02	<b>A1</b> .	(43) International Publication Date: 16 October 1997 (16.10.97)

US

(21) International Application Number: PCT/US97/04527

(22) International Filing Date: 4 April 1997 (04.04.97)

5 April 1996 (05.04.96)

(60) Parent Application or Grant

(63) Related by Continuation

US Filed on

(30) Priority Data: 08/628,773

> 08/628,773 (CIP) 5 April 1996 (05.04.96)

(71) Applicant (for all designated States except US): DEPUY ORTHOPAEDICS, INC. [US/US]; 700 Orthopaedic Drive, P.O. Box 988, Warsaw, IN 46581-0988 (US).

(72) Inventors; and

(75) Inventors/Applicants (for US only): PLOUHAR, Pamela, L. [US/US]; 17411 Battles Road, South Bend, IN 46614 (US). DUNN, Michael, D. [US/US]; 109 Third Street, Winona Lake, IN 46590 (US). LOWER, Jerry, L. [US/US]; 350 18th Road, Bourbon, IN 46504 (US). MAY, Thomas, C. [US/US]; 1511 Kings Highway, Winona Lake, IN 46590 (74) Agents: COFFEY, William, R. et al., Barnes & Thomburg, 1313 Merchants Bank Building, 11 South Meridian Street, Indianapolis, IN 46204 (US).

(81) Designated States: CA, JP, US, European patent (AT, BE, CH, DE, DK, ES, FI, FR, GB, GR, IE, IT, LU, MC, NL, PT,

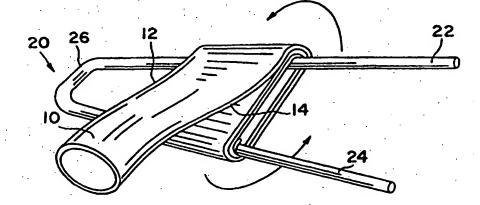
Published

With international search report.

(54) Title: TISSUE GRAFT CONSTRUCT FOR REPLACEMENT OF CARTILAGINOUS STRUCTURES

#### (57) Abstract

A method of forming a reconstructive structure for cartilaginous elements, and the product produced by that method is disclosed. A length of small intestine submucosa tissue (10) is wrapped around a mandril (20) having legs (22 and 24) connected a bight (26) and diverging from that point. The diverging angle of the legs (22 and 24) of the mandril is selected to compensate for various lengths of the edges (12 and 14) and to produce flat or planar layers. The multilayered composite produced is used in the repair or replacement of cartilaginous tissues.



**Best Available Copy** 

#### FOR THE PURPOSES OF INFORMATION ONLY.

Codes used to identify States party to the PCT on the front pages of pamphlets publishing international applications under the PCT.

AL	Albania	ES	Spain	LS	Lesotho	SI	Slovenia
AM	Armenia	FI	Finland	LT	Lithuania	SK	Slovakia
AT	Austria	FR	France	LU	Luxembourg	SN	Senegal
AU	Australia	GA	Gabon	LV	Latvia	SZ	Swaziland
AZ .	Azerbaijan	GB	United Kingdom	MC	Monaco	TD	Chad
BA	Bosnia and Herzegovina	GE	Georgia	MD	Republic of Moldova	TG	Togo
BB	Barbados	GH	Ghana	MG	Madagascar	TJ	Tajikistan
BE	Belgium	GN	Guinea	MK	The former Yugoslav	TM	Turkmenistan
BF	Burkina Paso	GR -	Greece		Republic of Macedonia	TR	Turkey
BG	Bulgaria	HU	Hungary	ML	Mali	TT	Trinidad and Tobago
BJ	Benin	IE	Ireland	MN	Mongolia	UA	Ukraine
BR	Brazil	IL.	Israel	MR	Mauritania	UG	Uganda
BY	Belarus	IS	Iceland	MW	Malawi	US	United States of America
CA	Canada	IT	Ítaly	MX	Mexico	UZ	Uzbekistan
CF	Central African Republic	JP	Japan	NE	Niger	VN	Viet Nam
CG	Congo	KE	Kenya	NL	Netherlands	YU	Yugoslavia
CH	Switzerland	KG	Kyrgyzstan	· NO	Norway "	zw	Zimbabwe
CI	Côte d'Ivoire	KP .	Democratic People's	NZ	New Zealand		
СМ	Cameroon		Republic of Korea	PL	Poland		
CN	China	KR	Republic of Korea	PT	Portugal		•
CU	Cuba	KZ	Kazakstan	RO	Romania		
CZ	Czech Republic	LC	Saint Lucia	RU	Russian Federation		
DE	Germany	u	Liechtenstein	SD	Sudan		
DK	Denmark	LK	Sri Lanka	SE	Sweden		
EE	Estonia	a LR	Liberia	SG	Singapore		
		. 6 %	· / / / ·		-		
l			* * * * * * * * * * * * * * * * * * * *		*		•

WO 97/37613 PCT/US97/04527

# TISSUE GRAFT CONSTRUCT FOR REPLACEMENT OF CARTILAGINOUS STRUCTURES

#### Background and Summary of the Invention

The present invention relates generally to cartilaginous reconstruction and more specifically to a method of forming a reconstructive structure for cartilage elements, reconstructing a cartilage element in situ using the reconstructive structure and reconstructing a joint having two bones separated by cartilage material.

Researchers in the surgical arts have been working for many years to develop new techniques and materials for use as grafts to replace or repair damaged or diseased tissue structures, particularly bones, cartilaginous tissue and connective tissues, such as ligaments and tendons, and to hasten fracture healing. It is very common today, for instance, for an orthopaedic surgeon to harvest a patellar tendon of autogenous or homologous origin for use as a replacement for a torn cruciate ligament. The surgical methods for such techniques are well known. Further, it has become common for surgeons to use implantable prostheses formed from plastic, metal and/or ceramic material for reconstruction or replacement of physiological structures.

It has been reported that compositions comprising the submucosa of the intestine of warm-blooded vertebrates can be used as tissue graft materials in sheet form. See U.S. Pat. No. 4,902,508. The preferred sheet compositions described and claimed in that patent are characterized by excellent mechanical properties, including high compliance, a high burst pressure point, and an effective porosity index which allowed such compositions to be used beneficially for vascular graft constructs.

The graft materials disclosed in that patent are also useful in tendon and ligament replacement applications as described in U.S. Pat. No. 5,281,422. When used in such applications the graft constructs appear to serve as a

35

15

20

matrix for the growth of the tissues replaced by the graft constructs. When used in cruciate ligament replacement experiments not only does the portion of the graft traversing the joint become vascularized and actually grow to look and function like the original ligament, but the portion of the graft in the femoral and tibial bone tunnels rapidly incorporates into and promotes development of the cortical and cancellous bone in those tunnels. It was believed that such properties derived from the sheet structures of the intestinal tissue derived graft constructs. U.S. Pat. No. 5,281,422 also describes in Figs. 8 and 9 doubling the graft back over itself, one layer on top of the other or rolling it concentrically, one layer on top of the other.

An advantage of the intestinal submucosa graft formed for surgical repair is its resistance to infection. The intestinal graft material, fully described in the aforesaid patents, have high infection resistance, long shelf life and storage characteristics. It has been found that xenogeneic intestinal submucosa is compatible with hosts following implantation as vascular grafts, ligaments and tendons and is not recognized by the hosts' immune system as "foreign" and therefore is not rejected.

As described in U.S. Pat. No. 5,275,826, fluidized
intestinal submucosa can be injected into host tissues in need of repair, for example, bone and soft tissue such as muscle and connective tissues. Also described is the surgical reconstruction of a collagenous meniscus at the interface of articulating bones. In such reconstruction a sheet of a first tissue graft composition, preferably itself comprising intestinal submucosa of a warm-blooded vertebrate, is formed into a sealed pouch and filled with the fluidized tissue graft composition of intestinal submucosa.

The present invention is directed to multi-layered tissue graft constructs and a method of preparing those

graft constructs. The intestinal submucosa tissue graft constructs of the present invention are utilized in the reconstruction of damaged or diseased cartilaginous structures. In one embodiment, a method is provided for the *in vivo* reconstruction of a cartilaginous structure, or for the reconstruction of a joint having two bones separated by cartilaginous material.

The method of repairing damaged or diseased cartilaginous structure in vivo is achieved by a reconstructive tissue graft structure or construct that includes a plurality of superimposed layers of intestinal submucosa tissue compressed and secured together and shaped to provide a solid multi-layer reconstructive element of the anatomical shape of the cartilaginous element to be reconstructed. The reconstructed structure is formed by 15 superimposing a plurality of layers of small intestinal submucosa and securing the layers to one another. embodiment, the superimposed layers are compressed and secured together. The compressed and secured solid multilayered structure is cut, and optionally sculptured, to form a reconstructive structure having the anatomical shape of the cartilaginous structure to be replaced.

The superimposed layers may be formed by wrapping a continuous piece of small intestinal submucosa about a pair of spaced mandrels. Preferably, the mandrels are positioned to diverge at an acute angle from an apex. This allows the concave edge of the small intestine submucosa to be closer to the apex than the concave edge and therefore compensate for the varying edge length of the small intestine submucosa. This results in a substantially planar structure of the multi-layers. Alternatively, small intestine submucosa is cut into sheets and the sheets are superimposed or stacked. The angular orientation of the sheets in parallel plane may be varied.

A clamp or other tool or hydraulic press may be used to compress the superimposed layers together and hold them



while they are secured together. The layer may be secured together by stitching, crimping, quilting, drying or drying in a vacuum.

The clamp may include a slot which serves as a suturing guide. Also, the outline of the clamp may be used as a cutting guide. In addition to cutting the outline of the desired anatomical shape, the multi-layers may be sculptured in the cross-section to the desired anatomical shape.

The reconstructive structure just described may be 10 used for reconstructing a cartilaginous element in situ. The method includes removing at least a portion, if not substantially all of the cartilaginous element, but leaving a seed portion, sculpting a reconstructive structure formed of plural layers of small intestine submucosa to the 15 anatomical shape of the cartilaginous element being reconstructed, and positioning it adjacent to the seed portion of the cartilaginous element. The reconstructive element is secured to the seed portion of the cartilaginous element such that the reconstructive structure forms the 20 substrate for endogenous cartilage growth from the seed portion.

A method for reconstructing a joint having two bones separated by a cartilaginous material includes removing any remaining portion of the cartilaginous material down to a bleeding bone site. A reconstructive structure formed of small intestine submucosa is positioned adjacent to the bleeding bone site and secured to the bleeding bone site so that the reconstructive structure forms a substrate for cartilaginous growth from the bleeding bone site. This provides a cartilaginous layer of material on the bone site. As an alternative, a membrane or barrier may be inserted to cover the area of the bleeding bone and the reconstructive element may be affixed to the membrane or barrier.

If a sufficient amount of cartilaginous material remains on the bone, the cartilage can be abraded to create a uniform defect without taking it to the bleeding bone. A reconstructive element is then attached to the remaining cartilaginous material.

Other objects, advantages and novel features of the present invention will become apparent from the following detailed description of the invention when considered in conjunction with the accompanying drawings.

10

15

20 -

30.

#### Brief Description of the Drawings

Fig. 1 is a perspective view of a mandril and method of forming a plurality of layers of small intestinal submucosa according to the principles of the present invention;

- Fig. 2 is a perspective view of a clamping tool and guide according to the principles of the present invention;
- Fig. 3 is a plan view of a method of clamping and securing according to the principles of the present invention;
- Fig. 4 is a perspective view of cutting the clamped plural layers using the clamp as a guide;
- Fig. 5 is a perspective view of the cutting step without a guide;
- 25 Fig. 6 is a perspective view of the method of preparing the site and attaching the reconstructive structure according to the principles of the present invention;
  - Fig. 7 is a perspective view of a backbone;
  - Fig. 8 is a cut-away perspective view of a wrist;
    - Fig. 9 is another cut-away view of a wrist;
    - Fig. 10 is a cut-away view of a shoulder;
  - Fig. 11 is a view of a second embodiment forming a plurality of layers from sheets of small intestinal submucosa according to the principles of the present invention;

30

35



Fig. 12 is a diagrammatic view of another method of clamping and securing according to the principles of the present invention; and

Fig. 13 is a perspective view of the method of securing using quilting according to the principles of the present invention.

## Detailed Description of the Preferred Embodiments

The starting material for the structure in accordance with the present invention comprises vertebrate submucosa, 10 most preferably, the tunica submucosa along with a basilar portion of the tunica mucosa of a segment of intestinal tissue of a warm-blooded vertebrate. One preferred starting material comprises the tunica submucosa along with 15 the lamina muscularis mucosa and the stratum compactum of a segment of small intestine, said layers being delaminated from both the tunica muscularis and the luminal portion of the tunica mucosa of said segment. Such a material is referred to herein as Small Intestine Submucosa ("SIS"). The thickness and definition of the basilar components of 20 the tunica mucosa, i.e., the lamina muscularis mucosa and the stratum compactum, are known to be species dependent.

The preparation of SIS from a segment of small intestine is detailed in U.S. Pat. No. 4,902,508, the disclosure of which is expressly incorporated herein by reference. A segment of intestine, preferably harvested from porcine, ovine or bovine species, is first subject to abrasion using a longitudinal wiping motion to remove both the outer layers (particularly the tunica serosa and the tunica muscularis) and the inner layers (at least the luminal portions of the tunica mucosa). Typically, the SIS is rinsed with saline and optionally stored in a hydrated or dehydrated state until use as described below.

In accordance with one embodiment, a tissue graft construct is formed for the replacement or repair of an endogenous cartilaginous structure. The method comprises

the steps of superimposing a plurality of layers of intestinal submucosa and securing the layers together to form a multi-layered construct and cutting the secured layers into the anatomical shape of the cartilagineous structure to be replaced or repaired. The multilayered constructs are provided with a sufficient number of submucosal tissue layers to form a reconstructive tissue graft construct having the desired thickness for the replacement of the endogenous cartilaginous structure. shape and thickness of the tissue graft construct is varied depending on the cartilaginous structure to be replaced, however the multi-laminate constructs typically range from about 10 to about 300 layers with the final construct having a thickness of about 1 to about 12 mm. 15 embodiment the tissue graft construct comprises about 25 to about 200 layers of submucosa tissue and has a final thickness of about 2 to about 8 mm. In another embodiment the tissue graft construct comprises about 50 to about 300 layers of submucosa tissue and has a final thickness of 20 about 4 to about 12 mm.

The graft constructs of the present invention can be formed for the replacement and repair of the articular cartilage of a joint, a meniscus shaped cartilaginous element or an intervertebral disc. In particular, graft constructs formed for the replacement of the articular cartilage of joints typically comprise about 10 to about 100 layers and have a thickness ranging from about 1 to about 4 mm. In one embodiment an articular cartilage graft construct comprises about 20 to about 100 layers of 30 submucosa tissue and has a thickness of about 2 to about 4 Tissue graft constructs formed for the replacement of a meniscus shaped cartilaginous element typically comprise about 50 to about 200 layers and have a thickness ranging from about 4 to about 8 mm. In one embodiment a meniscus construct comprises about 100 to about 200 layers of submucosa tissue and has a thickness of about 5 to about 8 Tissue graft constructs formed for the replacement of a spinal intervertebral disc typically comprise about 50 to

10

15

20

25

30

35

about 300 layers and have a thickness ranging from about 4 to about 12 mm. In one embodiment a intervertebral disc graft construct comprises about 100 to about 300 layers of submucosa tissue and has a thickness of about 5 to about 12 mm.

The layers of submucosa tissue are secured to one another by conventional techniques known to those skilled in the art and include, for example, the use of sutures, adhesives, staples and drying the tissue. In one embodiment the layers of intestinal submucosa are compressed while the layers are secured. In one embodiment the layers are compressed utilizing a clamp, and more preferably using a clamp that is in the shape of the cartilaginous structure to be replaced. The clamp can be utilized as an outline for cutting the shape of the graft construct or the clamp itself is used as a die in a press.

In accordance with one embodiment the submucosa layers are secured by drying the layers while compressing the intestinal submucosa. In addition, a vacuum can be applied to overlapped layers of tissue during the drying process. Furthermore, heat can be applied to the tissue graft during the compression of the intestinal submucosa to speed the drying process.

The tissue graft constructs of the present invention are utilized to replace or repair cartilaginous structures of vertebrate species. The tissue graft construct comprise a plurality of layers of intestinal submucosa superimposed and secured together to form a multi-layered construct. A sufficient number of submucosal layers are overlaid to form a multi-layered construct having a thickness of about 1 to about 12 millimeters. Typically about 10 to about 300 layers are used, depending on the thickness of the individual layers. The multi-layered construct is then cut and sculptured to form the desired three dimensional anatomical shape of the cartilagineous structure to be replaced or repaired. In accordance with one embodiment the multi-layered construct is formed to have a thickness of about 4 to about 8 millimeters and is cut and sculptured

25

30

in the shape of a meniscus. In another embodiment the multi-layered construct is formed to have a thickness of about 1 to about 4 millimeters and is cut and sculptured in the shape of the articular cartilage of a joint. another embodiment the multi-layered construct is formed to have a thickness of about 5 to about 12 millimeters and is cut and sculptured in the shape of an intervertebral disc.

In accordance with one embodiment the multilayered construct can be rapidly formed as a solid graft construct by wrapping a continuous piece of intestinal submucosa about a pair of spaced mandrels, securing the layers together, and cutting the secured layers into the desired anatomical shape. This method speeds the preparation of the tissue constructs by eliminating the steps of cutting the submucosa tissue into sheets of tissue. In one preferred method, the tissue graft constructs are formed by wrapping a continuous piece of intestinal submucosa about a pair of spaced mandrels, wherein the intestinal submucosa is in the form of a tube 20 having a concave and a convex lateral edge, and the mandrels are positioned to diverge at an acute angle from an apex. In this embodiment the submucosa tissue tube is wrapped onto the mandrels with the concave edge closer to the apex than the convex edge.

The method of forming a reconstructive structure for cartilaginous elements will be described specifically for a meniscus shaped cartilaginous element as an example. Specifically as discussed with respect to Fig. 6, it will be the meniscus in the knee joint.

As illustrated in Fig. 1, a length of SIS 10 is wrapped around a mandril 20 having legs 22 and 24 connected at bight 26 and diverging therefrom. The SIS 10 includes two lateral edges 12 and 14 of different lengths. This is a natural condition of the material and may be considered a concave shorter or mesenteric edge 12 and a convex longer or anti-mesenteric edge 14. The diverging angle of the legs 22 and 24 of the mandril is selected to compensate for the various lengths of the edges 12 and 14 and to produce

10

15

20

25

30

flat or planar layers. Without the mandril 20, the superimposed layers would have a tendency to buckle or the SIS would have to be stretched and thereby producing uneven tension on the surface. Once the number of layers required to duplicate the cartilaginous element to be replaced have been wrapped on the mandrel 20, the layers are compressed or clamped together for securing.

Tool 30, illustrated in Fig. 2, includes a pair of arms 32 pivotally connected together and terminating in templates or clamping heads 34. The clamping heads 34 have an exterior shape of the cartilaginous element to be reconstructed. The arms 32 of the clamp 30 may include interlocking projections 38 as in other surgical or medical clamps. As previously discussed, this is a menistus shape. Each head 34 includes a slot 36 which is a guide for suturing the layers together.

As illustrated in Fig. 3, the clamp 30 is applied to the plurality of the layers of SIS 10 while on the mandrel 20. One method of securing includes using a needle 40 and suture 42 to suture through the slot 36 in the template 34. Alternative methods of securing the layers together is quilting, crimping, drying and drying under a vacuum. All of these are performed while compressing the layers using the clamp 30 or other shape or style of compression plates or devices or hydraulic pressure.

The secured layers are then shaped by cutting with a knife 46 as illustrated in Fig. 4. Preferably, the clamping heads 34 form a template for the cutting as illustrated in Fig. 4. The complete meniscus shape may be cut using the heads 34 as a template or only one side thereof with the remainder being cut freehand as illustrated in Fig. 5. Alternatively, the clamp heads 34 may have a peripheral projection and used as a die in a press to cut the layers to the desired shape.

Also, since meniscus and other shapes do not have uniform cross-sections, the sculpturing of the resulting

structure 16 may be performed using the knife 46. Sculpturing is intended to include the original cutting as well as cross-sectional shaping. Thus, a flat planar construct illustrated in Fig. 5 may be provided by the surgeon, who then sculptures it to replicate substantially the exact shape of the meniscus required for the appropriate patient.

As an alternative method of forming a plurality of superimposed planar layers of SIS, the SIS 10 may be cut along its length and then cut into an appropriate size sheets. As illustrated in Fig. 11, the SIS 10 may be cut along its concave or shorter edge 12 such that the convex or longer edge 14 is in the center of the strip. This particular selection of cutting minimizes the variation in size and tension and increases the planarity. 15 Depending upon the diameter of the SIS, it will have a width of approximately 1-2 inches (2.56-5.12 cm.). The SIS will then cut into sheets or segments 18, for example, 2-3 inches (5.12-7.68 cm.) long. Other methods to form the 20 sheets may be used.

To further remove or compensate for any variance in the individual sheets 18, the sheets may have varying angular orientation as they are stacked, as illustrated in Fig. 11.

As an alternative to the securement of suturing of Fig. 5, the plurality of superimposed layers of SIS may be compressed between a pair of compressor plates 33 in a heating chamber 35 as illustrated in Fig. 12. This dries the compressed structure 16 and secures the plurality of layers of SIS together. The chamber 35 may be a pressurized chamber and may either increase the pressure above atmosphere or form a vacuum. A construct 16 has been formed by applying twenty pounds of pressure by the pressure plates 33 and heating at 40°C for between 48-72 hours. Additional experiments have been conducted wherein the construct 16 is dried in a vacuum at ambient

15

20

temperature, from 72 to 96 hours. The temperature may vary from ambient to 50°C. The pressure from a vacuum to 40 psi and time may vary to produce desired construct 16. The parameters are selected to prevent delamination of the plurality of layers 18 of the construct 16 while producing the desired density of the ultimate product. The number of layers may vary between 50, for example, to about 200 layers, depending upon the thickness of the individual layers, so as to produce an ultimate construct 16 having a thickness, for example, of 4-8 millimeters.

As a further alternative, the plurality of layers of SIS may be secured by quilting as illustrated by the quilting pattern 43 in Fig. 13. The quilting may be produced either before, during or after drying on pressing. If performed during pressing using pressing plates, an appropriate opening must be provided in the pressing plate 33. Other methods of securing may be used. It is preferred that the securement be performed while the plurality of superimposed layers of SIS are being compressed.

As an example, the thickness of the meniscus in the knee joint may vary between four to eight millimeters in an individual, for example. Thus, a replacement reconstructive structure would include between 50 to 200 layers or more, depending upon the method of forming the 25 structure 16. The reconstructive structure 16 of Figure 5 is a solid multi-layer reconstructive structure having the anatomical shape of the cartilaginous element to be reconstructed. By providing the general shape of the uniform layers of SIS, sculpturing for the individual 30 application may be achieved. Securing with suture 44 along the larger exterior radius of the structure 16 permits the securing of the elements of the unified structure and sculpturing along the other edges depending upon the structure of the bones to which the cartilaginous element 35 is to be inserted.

The method of reconstructing a cartilaginous element in situ will be described in Fig. 6 with reference to a meniscus at the knee joint. Although the femur 50 is shown separated from the tibia 52 for sake of clearer

- illustration of the invention, the method includes minimum invasive surgery without the separation of the femur 50 and the tibia 52. The lateral and medial condyle of the femur 50 and the lateral and medial facet of the tibia include articular surfaces 51 and 52 respectfully of cartilaginous material. The cartilaginous material 51 and 53 are separated by medial meniscus 54 and lateral meniscus 55 which are secured by ligaments to the femur 50 and tibia 52. A portion of securing ligaments 56 and 57 for the meniscus 54 and 55 are shown.
- At least the portion, if not substantially all, of a damaged cartilaginous element or meniscus 54 is removed. Preferably, a seed portion remains. If a small crescent shape is not damaged and remains, it will provide an attachment section for the reconstructive element 16 as well as a seed for the growth of the replacement cartilaginous element. Also, by leaving a crescent shape portion, the ligaments then can be used to hold the remainder of the meniscus to the bone. The replacement cartilaginous element 16 has been attached by suturing, using needle 47 and suture 48 to the remaining portion as illustrated for the lateral meniscus 55.

If the cartilaginous element or meniscus 54 is not damaged beyond repair, but only torn, small portions of the damaged cartilaginous element can be removed and 30 replacement cartilaginous element 16 attached thereto. Alternatively, a replacement cartilaginous element 16 is sculptured to represent the damaged layers and attached directly to the in situ cartilaginous element or meniscus 54. This will strengthen the torn element without removing it. As discussed above, appropriate sculpturing is performed.

10

As previously discussed, the surgery is performed by minimal invasion from the side of the joint. Well known methods of cutting and suturing may be performed. If the meniscus 54 and 55 is so damaged such that a continuous crescent shape is not available for attaching, the reconstructive structure 16 may be attached to the tendon 56, 57 by any remaining seed section. The seed portion of the meniscus 54, 55 in combination with the synovial fluids support the growth of cartilaginous material using the SIS as a matrix or substrate.

The reconstructive structure of the present invention can also be used to repair, in situ, the articulation cartilage 51 and 52 on the surface of the femur 50 or tibia The reconstructive structure induces the production of hyaline cartilage. The areas where the method is used is 15 the tibia plateau, the femoral condyle, the femoral head and acetabula, ankle joint, elbow joint, shoulder joint, finger joints. The desired thickness of the SIS structure 16 is provided and secured to the bone by suturing or 20 tissue adhesive, for example, fibrin glue. The damaged cartilaginous material is scraped down to a bloody surface of the bone to allow the necessary seed site for the growth of the cartilaginous material. Alternatively, a membrane or barrier may be inserted to cover the area of the bleeding bone, and the reconstructive element is affixed to 25 that membrane or barrier. A barrier is used to separate the bleeding bone from the reconstructive element, for example, and may include ceramic or a resorbable membrane. The membrane is secured by tacking or any other method. the cartilaginous material on the bone is not substantially 30 damaged, the cartilage is abraded to create a uniform damaged area without taking it to the bleeding bone. reconstructive element is then attached to the remaining cartilaginous material by suturing or using a tissue 35 adhesive.

The same process may be used to replace intervertebral disc. As illustrated in Fig. 7, the vertebral body 62 is separated by intervertebral disc 64 of cartilaginous material. Reconstruction of an intervertebral disc 64 can 5 be accomplished according to the method described with respect to Fig. 6 by attaching the SIS shaped disc to a remaining undamaged disc portion. Alternatively, fusion may take place between the adjacent vertebral body 62. The broken or split intervertebral disc 64 is removed down to a bleeding bone. The reconstructive structure of SIS formed by the method described to Figs. 1-5 or 11-13 is inserted between the vertebral body 62. The bloody bone becomes the seed site and the SIS reconstructive structure forms a matrix for forming a bony structure. This is an example of a fibrocartilage structure. Other formations of the fibro structure would be the symphysis pubis mandibular joint and sterno clavicular joint.

Other types of cartilage or elastic cartilage is used in reconstructive surgery to model facial features such as nose and ears. The reconstructive structure formed according to the method of Figs. 1-5 may be used for the substrate or reconstruction of elastic cartilage.

As illustrated in Fig. 8, a cartilaginous meniscus 70 and articular disc 72 in the wrist may be restructured using the present method. Similarly, as illustrated in Figure 9, the radiocarpal articulation 74 and the intercarpal articulation 76 in the hand may also be reconstructed using the method of the present invention.

As illustrated in Fig. 10, the articular cartilage 80 on the humerus 82 rides on the cartilage 84 in the glenoid cavity of the scapula 86. Both the articular cartilage 82 and the cartilage of the glenoid cavity 84 may be replaced using the method of the present invention.

Although the present invention has been described and illustrated in detail, it is to be clearly understood that the same is by way of illustration and example only, and is

20

25

30

not to be taken by way of limitation. The spirit and scope of the present invention are to be limited only by the terms of the appended claims.

#### CLAIMS:

1. A method of forming a tissue graft construct for replacement or repair of a cartilaginous structure, said method comprising:

superimposing a plurality of layers of intestinal submucosa and securing the layers together to form a multi-layered construct having a thickness of about 1 to about 12 millimeters; and

cutting the secured layers to form the anatomical shape of the cartilagineous structure to be replaced or repaired.

- 2. The method of claim 1, wherein said tissue graft construct comprises about 50 to about 300 layers.
- 3. The method of claim 1, wherein said tissue graft construct comprises about 50 to about 200 layers.
- 4. The method of claim 1, wherein said layers of intestinal submucosa are compressed while the layers are secured.
- 5. The method of claim 4, wherein said layers are compressed with a clamp.
- 6. The method of claim 5, wherein said clamp includes a slot used as a suturing guide.
- 7. The method of claim 5, wherein a portion of said clamp is used as a cutting guide.
- 8. The method of claim 1, wherein said method includes cutting the secured layers to conform to an outline of the anatomical shape and sculpturing the resulting planar construct to the desired shape in cross section.
- 9. The method of claim 1, wherein said multi-layered construct is cut in the shape of a meniscus.
- 10. The method of claim 1, further comprising the step of cutting said intestinal submucosa into sheets, wherein each sheet forms a layer of the tissue graft construct.
- 11. The method of claim 5, wherein said layers are cut using said clamp as a die in a press.

- 12. The method of claim 1, wherein said layers are secured by drying said layers while compressing the intestinal submucosa.
- 13. The method of claim 12, further comprising the step of applying heat during the compression of the intestinal submucosa.
- 14. The method of claim 1, wherein said layers are secured by drying said layers while applying a vacuum.
- 15. The method of claim 1, wherein said layers are secured by sutures.
- 16. A method of forming a tissue graft construct for replacement or repair of cartilaginous tissues, said method comprising:

wrapping a continuous piece of intestinal submucosa about a pair of spaced mandrels to form a multi-layered construct;

securing the layers together, and cutting the secured layers to form the anatomical shape of the cartilagineous structure to be replaced or repaired.

- 17. The method of claim 16, wherein said intestinal submucosa is in the form of a tube having a concave and a convex lateral edge, the mandrels are positioned to diverge at an acute angle from an apex, and the tube is wrapped onto the mandrels with the concave edge closer to the apex than the convex edge.
- 18. The method of claim 16, wherein said graft construct comprises about 50 to about 200 layers of intestinal submucosa.
- 19. The method of claim 16, wherein said tissue graft construct comprises about 50 to about 300 layers.
- 20. The method of claim 16, wherein the mandrels are wrapped with a sufficient number of layers to form a tissue graft construct having a thickness of about 1 to 12 millimeters.
- 21. The method of claim 16, wherein said layers are compressed while the layers are secured.

- 22. The method of claim 21, wherein said layers are compressed with a clamp.
- 23. The method of claim 22, wherein a portion of said clamp is used as a cutting guide.
- 24. The method of claim 22, wherein said layers are cut using said clamp as a die in a press.
- 25. The method of claim 16, wherein the step of securing the layers comprises drying said layers while compressing the layers.
- 26. The method of claim 16, wherein said layers are secured by sutures.
- 27. A method of forming a multi-layered tissue graft construct, said method comprising

preparing planar sheets of submucosal tissue; superimposing a plurality of said sheets; securing the layers together to form a tissue graft construct having a thickness of about 1 to about 12 millimeters; and

cutting the secured layers to form the anatomical shape of the cartilagineous structure to be repaired.

- 28. The method of claim 27, wherein said layers are secured to one another by sutures.
- 29. The method of claim 27, wherein said layers are secured to one another by drying said layers while compressing the submucosal tissue.
- 30. A tissue graft construct for the replacement or repair of a cartilaginous structure, said tissue graft construct comprising:

a plurality of layers of intestinal submucosa superimposed and secured together to form a multi-layered construct having a thickness of about 1 to about 12 millimeters, said multi-layered construct being cut and sculptured to the desired three dimensional anatomical shape of the cartilagineous structure to be replaced or repaired.

31. The tissue graft construct of claim 30, wherein said tissue graft construct comprises about 50 to about 300 layers.

- 32. The tissue graft construct of claim 30, wherein the tissue graft construct comprises about 50 to about 200 layers.
- 33. The tissue graft construct of claim 30, wherein the layers are compressed while the layers are secured.
- 34. The tissue graft construct of claim 30, wherein said multi-layered construct has a thickness of about 4 to about 8 millimeters and is cut and sculptured in the shape of a meniscus.
- 35. The tissue graft construct of claim 30, wherein said multi-layered construct has a thickness of about 1 to about 4 millimeters and is cut and sculptured in the shape of the articular cartilage of a joint.
- 36. The tissue graft construct of claim 30, wherein said multi-layered construct has a thickness of about 5 to about 12 millimeters and is cut and sculptured in the shape of an intervertebral disc.
- 37. A method of reconstructing a cartilaginous element *in situ* comprising:

removing a portion of a cartilaginous element, but leaving a seed portion;

positioning a reconstructive structure adjacent said seed portion, said reconstructive structure comprising a plurality of layers of intestinal submucosa tissue superimposed and secured together to form a multi-layered construct having a thickness of about 1 to about 12 millimeters, wherein the multi-layered construct is cut to form the anatomical shape of the cartilagineous structure to be reconstructed; and

securing said reconstructive structure to said seed portion.

38. The method of claim 37 further comprising the step of sculpturing the reconstructive structure to the three dimensional shape of the cartilaginous element being reconstructed before securing the reconstructive structure to the seed portion.

- 39. The method of claim 37, wherein said cartilaginous element is hyaline cartilage.
- 40. The method of claim 37, wherein said cartilaginous element is elastic cartilage.
- 41. The method of claim 37, wherein said cartilaginous element is fibrocartilage.
- 42. A method of reconstructing a joint having two bones separated by cartilaginous material, said method comprising:

removing any remaining portion of cartilaginous material down to a bleeding bone site;

positioning an anatomically shaped reconstructive structure, comprising multiple layers of intestinal submucosa and having a thickness of 1-12 millimeters, adjacent to said bleeding bone site; and

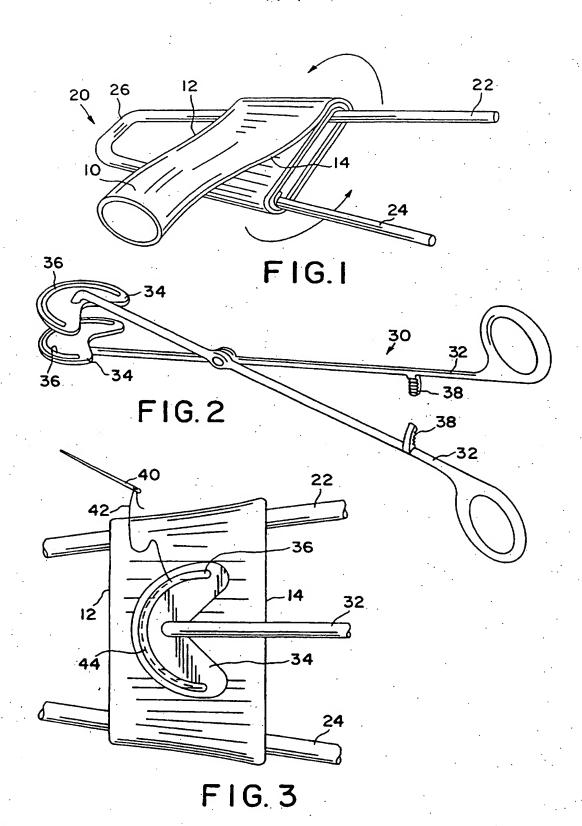
securing said reconstructive structure to said bleeding bone site.

- 43. The method of claim 42, wherein said cartilaginous element is hyaline cartilage.
  - 44. The method of claim 42, wherein said cartilaginous element is elastic cartilage.
  - 45. The method of claim 42, wherein said cartilaginous element is fibrocartilage.
  - 46. The method of claim 42, including sculpturing said reconstructive structure to the shape of the cartilaginous structure being reconstructed.
  - 47. The method of claim 42 including positioning a barrier layer between said bleeding bone site and said reconstructive structure, securing said barrier layer to said bone site and securing said reconstructive structure to said barrier layer.
  - 48. A method of reconstructing a joint having two bones separated by cartilaginous material comprising:

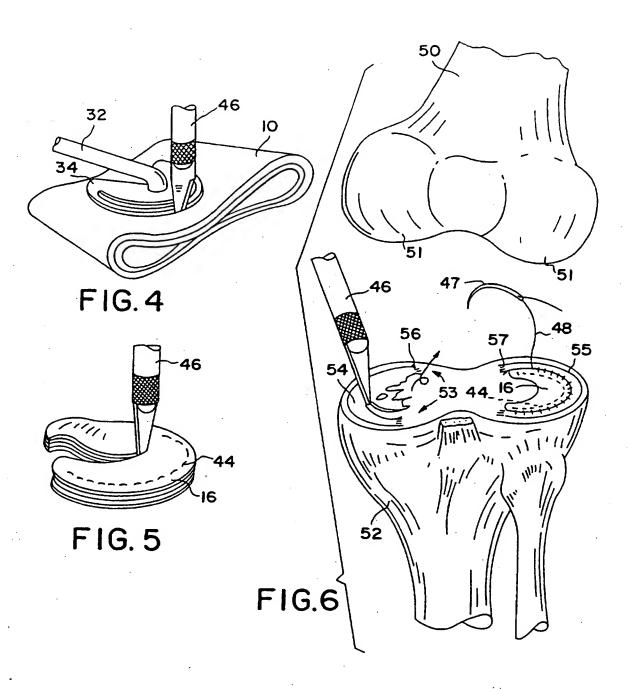
removing any remaining portion of cartilaginous material to create a defect site without creating a bleeding bone site;

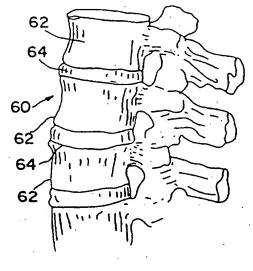
positioning an anatomically shaped reconstructive structure, comprising multiple layers of intestinal submucosa and having a thickness of 1-12 millimeters, adjacent to said bleeding bone site; and

securing said reconstructive structure to said bleeding bone site.



**SUBSTITUTE SHEET (RULE 26)** 





F1G. 7

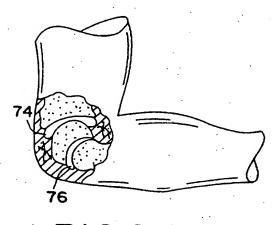


FIG.9

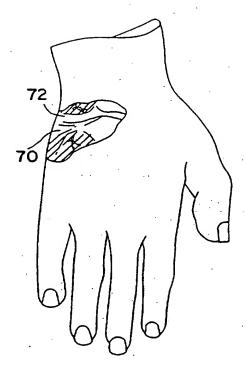
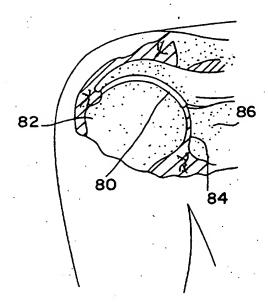
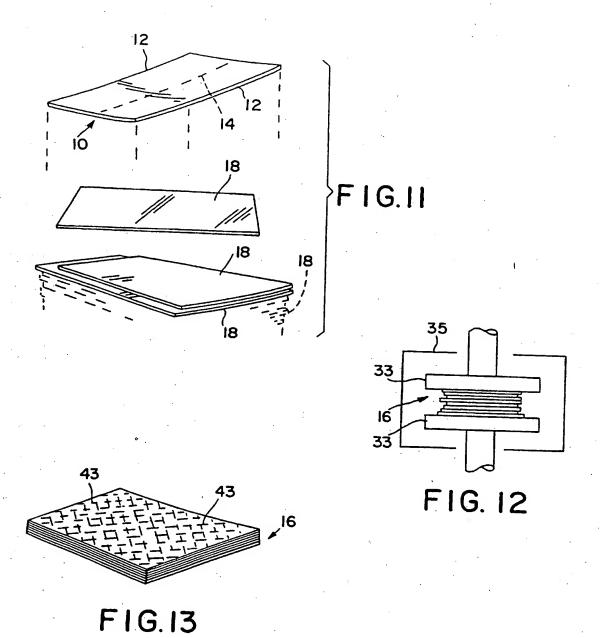


FIG.8



F I G. 10



SUBSTITUTE SHEET (RULE 26)

## INTERNATIONAL SEARCH REPORT

Form PCT/ISA/210 (second sheet)(July 1992)\*

Internal application No. PCT/US97/04527

A. CLASSIFICATION OF SUBJECT MATTER					
IPC(6) : A61F 2/02 US CL : 623/11		ļ			
According to International Patent Classification (IPC) or	to both national classification and IPC				
B. FIELDS SEARCHED	E. H I have be extraction combule.				
Minimum documentation searched (classification system	followed by classification symbols)	٠.			
U.S. : 623/11, 13, 901 600/36, 37					
Documentation searched other than minimum documenta	tion to the extent that such documents are included in the fields searched				
Electronic data hase consulted during the international s	earch (name of data base and, where practicable, search terms used)				
		٠. ا			
C. DOCUMENTS CONSIDERED TO BE RELE	VANT				
Category* Citation of document, with indication,	where appropriate, of the relevant passages Relevant to claim I	No.			
Y WO 95/06439 A (BOLESKY document.	) 09 March 1995, see the entire 1-5, 7-13, 1 and 27-36	5,			
Y US 4,585,458 A (KURLANI document.	D) 29 April 1986, see the entire 1-5, 7-13, 15 nd 27-36.	ō,a			
A US 3,562,820 A (BRAUN) 1 document.	6 February 1971, see the entire 1-48	,			
		•			
	·				
Further documents are listed in the continuation	of Box C. See patent family annex.				
Special categories of cited documents:	"T" later document published after the international filing date or prior date and not in conflict with the application but cited to understand	rity the			
"A" document defining the general state of the art which is not to be of particular relevance	considered principle of theory underlying the invention				
	Constitute of the design of the state of the				
(1.) document which may throw doubts on priority claim(s) of cited to establish the publication date of another citation special reason (as specified)	n or other  Y* document of particular relevance; the claimed invention cannot				
document referring to an oral disclosure, use, exhibition	considered to involve an inventive step when the document on or other combined with one or more other such documents, such combined being obvious to a person skilled in the art				
*P* document published prior to the international filing date by the priority date claimed					
Date of the actual completion of the international search	ch Date of mailing of the international search report				
03 JUNE 1997	11.06.97	· .			
Name and mailing address of the ISA/US Commissioner of Patents and Trademarks	Authorized officer Stacia Sinii	k.			
Hox PCF Washington, D.C. 20231	PAUL PREBILIC				
Facsunite No. (703) 305-3230	Telephone No. (703) 308-0858 X				





## WORLD INTELLECTUAL PROPERTY ORGANIZATION



#### International Bureau

INTERNATIONAL APPLICATION PUBLISHED UNDER THE PATENT COOPERATION TREATY (PCT)					
(51) International Patent Classification <sup>6</sup> :		(11) International Publication Number:	WO 97/37613		
A61F 2/02	A1	(43) International Publication Date:	16 October 1997 (16.10.97)		

PCT/US97/04527 (21) International Application Number:

(22) International Filing Date: 4 April 1997 (04.04.97)

(30)-Priority Data:

5 April 1996 (05.04.96) US 08/628,773

(60) Parent Application or Grant

(63) Related by Continuation

08/628,773 (CIP) UŚ Filed on 5 April 1996 (05.04.96)

(71) Applicant (for all designated States except US): DEPUY ORTHOPAEDICS, INC. [US/US]; 700 Orthopaedic Drive, P.O. Box 988, Warsaw, IN 46581-0988 (US).

(72) Inventors; and

(75) Inventors/Applicants (for US only): PLOUHAR, Pamela, L. [US/US]; 17411 Battles Road, South Bend, IN 46614 (US). DUNN, Michael, D. [US/US]; 109 Third Street, Winona Lake, IN 46590 (US). LOWER, Jerry, L. [US/US]; 350 18th Road, Bourbon, IN 46504 (US). MAY, Thomas, C. [US/US]; 1511 Kings Highway, Winona Lake, IN 46590 (US).

(74) Agents: COFFEY, William, R. et al.; Barnes & Thomburg, 1313 Merchants Bank Building, 11 South Meridian Street, Indianapolis, IN 46204 (US).

(81) Designated States: CA, JP, US, European patent (AT, BE, CH, DE, DK, ES, FI, FR, GB, GR, IE, IT, LU, MC, NL, PT, SE).

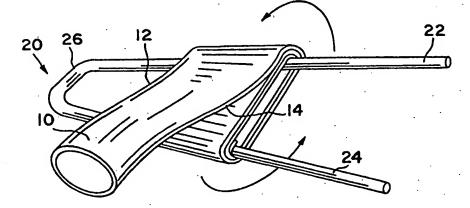
Published

With international search report.

(54) Title: TISSUE GRAFT CONSTRUCT FOR REPLACEMENT OF CARTILAGINOUS STRUCTURES

#### (57) Abstract

method of forming reconstructive structure for cartilaginous elements, and the product produced by that method is disclosed. A length of small intestine submucosa tissue (10) is wrapped around a mandril (20) having legs (22 and 24) connected a bight (26) and diverging from that point. The diverging angle of the legs (22, 24) of the mandril is selected to compensate for various lengths of the edges (12, 14) and to produce flat or planar layers. The multilayered composite produced is used in the repair or replacement of cartilaginous tissues.



## FOR THE PURPOSES OF INFORMATION ONLY

Codes used to identify States party to the PCT on the front pages of pamphlets publishing international applications under the PCT.

	•						-PP
AL	Albania	ES	Spain	LS	Lesotho	SI	Cl
AM	Armenia	FI	Finland	LT	Lithuania	SK	Slovenia
AT	Austria	FR	France	LU	Luxembourg		Slovakia
AU	Australia	GΛ	Gabon	LV	Latvia	SN	Senegal
ΑZ	Azerbaijan	GB	United Kingdom	MC	Monaco	SZ	Swaziland
BA	Bosnia and Herzegovina	GE	Georgia	MD		TD	Chad
BB	Barbados	GH	Ghana	MG	Republic of Moldova	TG	Togo
BE	Belgium	GN	Guinca	MK	Madagascar .	TJ	Tajikistan
BF	. Burkina Faso	GR	Greece	143 15	The former Yugoslav	TM	Turkmenistan
BG	Bulgaria	HU	Hungary	ML	Republic of Macedonia	TR	Turkey
BJ	Benin .	IE	Ireland	MN	Mali	TT	Trinidad and Tobago
BR	Brazil	IL	Israel	MR	Mongolia Mauritania	UA	Ukraine
BY	Belarus	IS	Iceland	MW		UG	Uganda
ÇA	Canada	IT	Italy	MX	Malawi Mexico	US	United States of Americ
CF	Central African Republic	JP	Japan	NE		UZ	Uzbekistan
CG	Congo	KE	Kenya	NL	Niger Netherlands	VN	Viet Nam
CH	Switzerland	KG	Kyrgyzstan	NO		YU	Yugoslavia
CI	Côte d'Ivoire	KP	Democratic People's	NZ	Norway	zw	Zimbabwe
CM	Cameroon		Republic of Korea	PL	New Zealand		
CN	China	KR	Republic of Korea	PT	Poland		
CU	Cuba	KZ	Kazaksian	RO	Portugal		
CZ	Czech Republic	LC	Saint Lucia	RU	Romania		
DE	Germany	Li	Liechtenstein	SD	Russian Federation		
DK	Denmark	LK	Sri Lanka		Sudan		
EE	Estonia	LR	Liberia	SE	Sweden		
			and it	SG ·	Singapore		

# This Page is Inserted by IFW Indexing and Scanning Operations and is not part of the Official Record

### **BEST AVAILABLE IMAGES**

Defective images within this document are accurate representations of the original documents submitted by the applicant.

Defects in the images include but are not limited to the items checked:

BLACK BORDERS

IMAGE CUT OFF AT TOP, BOTTOM OR SIDES

FADED TEXT OR DRAWING

BLURRED OR ILLEGIBLE TEXT OR DRAWING

SKEWED/SLANTED IMAGES

COLOR OR BLACK AND WHITE PHOTOGRAPHS

GRAY SCALE DOCUMENTS

LINES OR MARKS ON ORIGINAL DOCUMENT

REFERENCE(S) OR EXHIBIT(S) SUBMITTED ARE POOR QUALITY

## IMAGES ARE BEST AVAILABLE COPY.

□ OTHER: \_

As rescanning these documents will not correct the image problems checked, please do not report these problems to the IFW Image Problem Mailbox.

# THIS PAGE BLANK (USPTO)